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| Author | Family Name | Khan |
| | Particle | |
| | Given Name | Amjad |
| | Prefix | |
| | Suffix | |
| | Division | Faculty of Computer Science and Information Technology |
| | Organization | Universiti Malaysia Sarawak |
| | Address | 94300, Kota Samarahan, Sarawak, Malaysia |
| | Email | |
| Corresponding Author | Family Name | Iskandar |
| | Particle | |
| | Given Name | D. N. F. Awang |
| | Prefix | |
| | Suffix | |
| | Division | Faculty of Computer Science and Information Technology |
| | Organization | Universiti Malaysia Sarawak |
| | Address | 94300, Kota Samarahan, Sarawak, Malaysia |
| | Email | dnfaiz@unimas.my |
| Author | Family Name | Ujir |
| | Particle | |
| | Given Name | Hamimah |
| | Prefix | |
| | Suffix | |
| | Division | Faculty of Computer Science and Information Technology |
| | Organization | Universiti Malaysia Sarawak |
| | Address | 94300, Kota Samarahan, Sarawak, Malaysia |
| | Email | |
| Author | Family Name | Chai |
| | Particle | |
| | Given Name | Wang Yin |
| | Prefix | |
| | Suffix | |
| | Division | Faculty of Computer Science and Information Technology |
| | Organization | Universiti Malaysia Sarawak |
| | Address | 94300, Kota Samarahan, Sarawak, Malaysia |

Email

Abstract

Research on detecting, recognising and interpreting cardiovascular magnetic resonance images (CMRIs) has started since the 1980s. Time consuming and the need of expert evaluation are the key problems in the manual tracing efforts of CMRIs in a routine investigation. CMRIs manual tracing is also dependent on image quality, and there is no one-size-fits-all MRI setting for an optimum image result. In this paper, we present an approach using 2-Standard Division (2-SD) correlation along with the Sum of Absolute Difference technique and Otsu Watershed to automatically detect the left ventricle (LV) wall and blood pool in the effort to automatically assist the assessment of cardiac function. We test the approach using the Sunnybrook Cardiac Data, a standard benchmark dataset. The results shown that the proposed method had improved the automatic detection of the epicardium and endocardium.

Keywords
(separated by '-')

Cardiac MRI - Left ventricle - Automatic segmentation

Automatic Segmentation of CMRIs for LV Contour Detection

Amjad Khan, D.N.F.Awang Iskandar, Hamimah Ujir
and Wang Yin Chai

Abstract Research on detecting, recognising and interpreting cardiovascular magnetic resonance images (CMRIs) has started since the 1980s. Time consuming and the need of expert evaluation are the key problems in the manual tracing efforts of CMRIs in a routine investigation. CMRIs manual tracing is also dependent on image quality, and there is no one-size-fits-all MRI setting for an optimum image result. In this paper, we present an approach using 2-Standard Division (2-SD) correlation along with the Sum of Absolute Difference technique and Otsu Watershed to automatically detect the left ventricle (LV) wall and blood pool in the effort to automatically assist the assessment of cardiac function. We test the approach using the Sunnybrook Cardiac Data, a standard benchmark dataset. The results shown that the proposed method had improved the automatic detection of the epicardium and endocardium.

Keywords Cardiac MRI · Left ventricle · Automatic segmentation

1 Introduction

Cardiovascular disease (CVD) is a term for describing disease related to the heart or blood vessels and had been one of the major reasons of death all over the world [1]. For the past two decades, cardiovascular magnetic resonance (CMR) has emerged as an alternative noninvasive modality to assess and detect CVD. During a CMR scan, series of images are produced, and known as cardiovascular magnetic resonance images (CMRIs). These CMRIs depicts the valve anatomy that can be used for quantitative evaluation of stenosis and regurgitation.

The World Health Organisation (WHO) has listed CVD as one of the non-communicable diseases (NCDs) and currently part of the Global Action Plan for the

A. Khan · D.N.F.A. Iskandar (✉) · H. Ujir · W.Y. Chai
Faculty of Computer Science and Information Technology,
Universiti Malaysia Sarawak, 94300 Kota Samarahan, Sarawak, Malaysia
e-mail: dnfaiz@unimas.my

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24 Prevention and Control of NCDs 2013–2020 [1]. In conjunction with the action plan,
25 various semi-automatic and fully automatic techniques were developed to assess the
26 cardiac function and estimate cardiac parameters for clinical use. Common cardiac
27 parameters that are researched are ejection fraction (EF), end-systolic volume (ESV),
28 end-diastolic volume (EDV) and myocardial mass. CMRI has become a reference
29 examination for cardiac morphology, function and perfusion in humans. CMRI auto-
30 matic analysis is an open research due to the characteristics of CMR and variability
31 of the images among patients; the problem of cardiac cavity; weak edges informa-
32 tion; papillary muscles identification; and signal intensity.

33 Our research focuses on the mapping between CMRI and ontology to guide med-
34 ical decision making as it can be used to characterise the state and behaviour of
35 a patient’s disease both in terms of natural course and as the result of therapeutic
36 interventions. This paper presents part of our work in Phase 3, which is the auto-
37 matic detection of spatial regions in CRMI, described in Awang Iskandar et al. [2]. It
38 also contributes as phenomenon-centric data to support health care research. Besides
39 being part of the big data science research, transforming the data into knowledge
40 requires involvement of computer science techniques to aggregate the data in hierar-
41 chically organised knowledge that will be more understood by non-experts, such as
42 medical students and researchers from other domains.

43 CMRIs captures the space of liver, lungs, stomach and other surrounding organs.
44 The heart only comprises of approximately a 20% of the CMRI and left ventri-
45 cle (LV) takes comparatively less space. The LV is our region of interest in this
46 research. Semi-automatic methods use manual cardiac expert involvement to localise
47 LV detection and its walls. In this paper, we present a proposed approach to automati-
48 cally detect the left ventricle (LV) walls and compared the results against a reputable
49 research by Wijnhout et al. [3]. In particular we have improved the automatic detec-
50 tion of the epicardium and endocardium. One of the main challenges of automatic
51 segmentation of LV walls is the accuracy in segmenting the LV epicardium con-
52 tour due to the ballooning problem of the epicardium contours at the region between
53 myocardium and lung parenchyma.

54 The remainder of this paper is organised as follows. In Sect. 2, we present the
55 background on existing related work. In Sect. 3, we describe the proposed method.
56 In Sect. 4, we explain the benchmark dataset and experiment. In Sect. 5, we analyse
57 and evaluate the findings. We conclude in Sect. 6 along with our suggestions for
58 future work.

59 2 Related Work

60 Florentine et al. [4] recognized the problem with manual tracing efforts hampering
61 the adoption of cardiac MRI as routine investigation. Manual tracing is also depend-
62 ent on image quality, and there is no one-size-fits-all MRI setting for the optimum
63 image result. They compared results from a graph-based searching method with the
64 manual tracings, though they acknowledged that this in itself can be considered a
65 bias, as only decent images can be used. Attili et al. [5] recently reviewed the various

66 advances in CMRI image acquisition and processing. They remarked on the lack of
67 an integrated image analysis package for cardiac MRI, as the various solutions only
68 cater to selected elements within a cardiac MRI examination.

69 Research conducted to segment the LV walls automatically without expert inter-
70 vention and assessment of cardiac function involves several techniques including
71 fuzzy clustering [6]; dynamic programming [7]; active appearance model [8]; active
72 shape model [9]; deformable model [10]; graph cuts [11] image-driven approaches
73 [12] image-based methods(include region growing and thresholding [13]; pixel clas-
74 sification methods using classification and clustering [14] and atlas guided method
75 [15]. As the study of this segmentation method prove that the LV still need to deline-
76 ate accurate and fast automatic segmentation.

77 One of the most referred work for LV segmentation is done by Wijnhout et
78 al. [3] using a hybrid approach of active appearance model and active shape model.
79 Recently, Marino et al. [16] proposed a fully automated technique to detected points
80 inside the LV cavity; calculate the minimal biases and narrow limits of agreement for
81 LV volumes, ejection fraction and mass. On the other hand, Ringenberg et al. [17]
82 proposed a combination novel window-constrained accumulator thresholding tech-
83 nique to drive the segmentation of the right ventricular.

84 3 Automatic Segmentation of LV Walls

85 A CMRI slice is a series of images (in the form of video) that covers the whole car-
86 diac cycle, starting from systole to the end of systole; then from the start of diastole
87 to the end diastole. Existing research only manages to segment the LV walls from
88 one image of a slice [3], in our approach, we segmented all images in a slice and
89 render the motion along with the detected segmented walls. By accumulating the
90 information from the motion, segments and wall contours, we derive the LV func-
91 tion.

92 Before being able to estimate the LV function, an accurate delineation of the LV
93 walls is the primary task. In detecting the LV walls automatically—epicardium and
94 endocardium, the first step is to perform LV localisation to detect the LV from a
95 CMRI slice. We perform automatic region of interest (ROI) to detect the motion
96 areas of the block from CMR short axis (SAX) images. The roundness matrix was
97 used to draw the target circle around the LV ROI, we obtained the center point and
98 calculate the distance from the center point to the endocardium wall.

99 The second step is to segment and extract the epicardium and endocardium based
100 on the localised images. Besides segmenting the walls, this step also accurately
101 remove the papillary muscle and trabeculation from the contours of detected walls.
102 Otsu watershed was used to solve the heterogeneity problem in the blood pool. The
103 third step is to detect the wall contours in the CMRI slices. Here, we developed
104 an algorithm to locate the beating heart from the CRMIs and detect the motions
105 in a slice using the 2-Strandrad Division (2SD) correlation along with the Sum of
106 Absolute Differences technique. The 2SD is used to measure the similarity between
107 blocks of image by calculating the difference between each pixel of original image

108 to its corresponding pixel of the next image. Then absolutes of all differences are
 109 summed up. It results in a similarity block of simple metric form:

$$||D|| = \sum_{m=1}^n (||d||)$$

$$d = (x - y): x \in I, y \in T$$

110
 111 Here D is value of absolute differences and d is the difference of all pixels from I
 112 image and T the template image. If $x - y = 0$ then no difference is measured if $x - y >$
 113 0 then it means pixels have changed.

114 4 Experiment

115 We conducted an experiment to evaluate the effectiveness of the proposed approach.
 116 We used a standard benchmark dataset from the previous 2009 Cardiac MR Left
 117 Ventricle Segmentation Challenge [18]. It is also known as the Sunnybrook Cardiac
 118 Data, containing 45 cases in total. Among the 45 cases, 12 cases were heart failure
 119 with ischemia (HF-I), 12 cases of heart failure without ischemia (HF-NI), 12 cases of
 120 hypertrophy (HYP) and nine normal (N) cases. The image data were obtained during
 121 10–15 s breath-holds with a temporal resolution of 20 cardiac phases over the heart
 122 cycle. Six to twelve SAX images were obtained from the atrioventricular ring to the
 123 apex (with the specification of: thickness 58×10 mm, FOV $5320\text{mm} \times 320$ mm,
 124 matrix 5256×256). In particular, the cardiac cine MRI LV short axis slices were
 125 used for the experiment.

126 The proposed automatic method of segmenting the LV was tested on different
 127 patients each by using three different slices with 20 phases for each slice. Figure 1
 128 depicts a sample image of detected moving epicardium and endocardium contours
 129 that are highlighted in blue. The final endocardium border and contour detection
 130 (in Fig. 1III), uses the starting and ending points of the wall motion which provide
 131 accurate measures of LV.

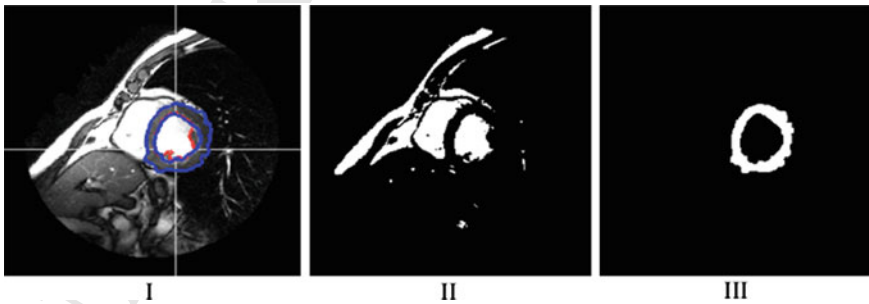


Fig. 1 I. Result of proposed automatic wall segmentation; II. Result of edge base detection for the walls; and III. Final endocardium border and contour detection. Best view in colour

Table 1 Comparison of contours detection results

| Patient_id | Wijnhout et al. [15] | | Proposed | |
|--------------------|----------------------|------------------|------------------|------------------|
| | Endocardium | Epicardium | Endocardium | Epicardium |
| SC-HF-I-05 | 100 | 100 | 100 | 100 |
| SC-HF-I-06 | 100 | 92 | 96.27 | 100 |
| SC-HF-I-07 | 75 | 100 | 88.35 | 100 |
| SC-HF-NI-31 | 84 | 100 | 94.57 | 100 |
| SC-HF-NI-33 | 89 | 90 | 89.55 | 100 |
| SC-HYP-06 | 85 | 100 | 86.34 | 100 |
| SC-HYP-07 | 69 | 100 | 84.65 | 100 |
| SC-HYP-08 | 68 | 90 | 80.52 | 92.20 |
| SC-HYP-37 | 85 | 86 | 85.46 | 400 |
| SC-N-05 | 80 | 100 | 93 | 100 |
| SC-N-06 | 92 | 86 | 94 | 100 |
| SC-N-07 | 78 | 80 | 95.32 | 100 |
| All(Mean \pm SD) | 83.75 \pm 10.51 | 93.66 \pm 7.22 | 90.24 \pm 5.83 | 99.35 \pm 2.25 |
| Overall | 90.37 \pm 21.62 | | 94.5 \pm 9.196 | |

132 5 Result Analysis and Evaluation

133 To analyse the effectiveness of the proposed algorithm, we evaluated the results
 134 against the measures available in Randau et al. [18]. Table 1 shows the result compar-
 135 ison between Wijnhout et al. [3] and the proposed approach—the good percentage of
 136 endocardium and epicardium contours that was successfully detected for the listed
 137 12 cases. A detail comparison with other known research will be presented in future
 138 publication. In this result, the patient ID SC-HF-I-08, SC-HF-NI-07 and SC-HF-NI-
 139 11 are missing because the proposed algorithm was designed for diastolic measure-
 140 ment and in these cases the automatic drawn contours are not able to detect the dias-
 141 tolic process due to the nature of the image collection in the dataset. On average the
 142 proposed approach detected 90.24 and 99.35 % of the endocardium and epicardium
 143 contours, respectively were detected within an average distance of 2.4 mm of the refer-
 144 enced manual contours. In most patient cases, the proposed approach managed to
 145 detect the endocardium better than Wijnhout's.

146 6 Conclusion and Future Work

147 To summarise, we have described a proposed approach for detecting LV walls. This
 148 approach is a pipeline of operations to perform LV localisation, LV segmentation
 149 and LV wall contour detection. With the aim to accurately perform an automatic

150 segmentation without human intervention using cardiac MRI images, the proposed
 151 approach shows a promising result of good contour detection of endocardium and
 152 epicardium contours for the assessment of cardiac function. Our future works include
 153 identification of similarity for clinical scoring, integrating data of temporal variations
 154 and knowledge representation model of semantics behind the cardiac functions.

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